1	Total kidney volume in autosomal dominant polycystic kidney disease:
2	intraobserver and interobserver agreement of two methods with MRI
3	Elif GÜNDOĞDU*, Çağatay CİHAN, Celal YAZICI
4	
5	Department of Radiology, Faculty of Medicine, Eskişehir Osmangazi University,
6	Eskişehir, Turkiye
7	
8	*Correspondence: elif_basbay@hotmail.com
9	
10	ORCIDs:
11	Elif GÜNDOĞDU: https://orcid.org/0000-0002-1729-6958
12	Çağatay CİHAN : https://orcid.org/0000-0002-8327-1302
13	Celal YAZICI: https://orcid.org/0000-0003-2376-1227
14	
15	Acknowledgment/disclaimers/conflict of interest
16	Conflict of interest: The authors have no conflicts of interest to declare.
17	Funding: The authors declare that no funds, grants, or other support were received
18	during the preparation of this manuscript.
19	Informed consent
20	The study was approved by the Ethics Committee of the Faculty of Medicine of
21	Eskişehir Osmangazi University (Date: 22.12.2021 No:E-25403353-050.99-266323).
22	The study was conducted in accordance with the principles of the Helsinki Declaration.
23	Datasets were evaluated retrospectively. Therefore, approval and informed consent were
24	not necessary and were waived by our local institutional review board.

Total kidney volume in autosomal dominant polycystic kidney disease: 1 2 intraobserver and interobserver agreement of two methods with MRI 3 Abstract 4 Background/Aim: Total kidney volume (TKV) is a parameter used in both treatment 5 decision and follow-up in autosomal dominant polycystic kidney disease (ADPKD) 6 patients. In this study, it was aimed to evaluate intraobserver and interobserver 7 agreement of the ellipsoid formula (EF) and manual boundary tracing method (MBTM) 8 used in TKV measurement of ADPKD patients in different levels of experience 9 radiologists, and also to evaluate the correlation between the EF and MBTM which is 10 considered the gold standard for TKV. Materials and methods: The magnetic resonance imaging (MRI) of 55 ADPKD 11 12 patients who underwent abdomen MRI between January 2017 and November 2021 for evaluating TKV were evaluated retrospectively. Measurements for TKV were 13 14 performed by three independent observers (observer 1, an abdominal imaging 15 radiologist with 5 years of experience; observer 2, a fourth-year radiology resident; observer 3, a second-year radiology resident). To assess intraobserver variability, all 16 observers repeated the measurements again at two week intervals. The ICC was used to 17 18 assess intraobserver and interobserver variability. Comparison of two methods was performed by linear regression for all three observers. 19 20 **Results:** The ICC (95% CI) indicated excellent agreement between the observers for both two methods (among all observers, p<0.001). Excellent intraobserver agreement 21 22 was found between all observer measurements either EF or MBTM based on ICC (95%

23 CI) (p<0.001). High correlations were observed for two methods in all 3 observers on

linear regression analysis (For first observer r=0.992, p<0.001; for second observer
 r=0.975, p<0.001; for third observer r=0.989, p<0.001).

Conclusion: Both of methods (EF and MBTM) using for measurement of TKV
provided excellent intra and interobserver reproducibility. The EF is as accurate and
precise as the MBTM. It can be preferred in radiology departments with heavy
workload because it is a reliable method for rapid and easy assessment independent of
experience.

Keywords: Autosomal dominant polycystic kidney disease, total kidney volume,
magnetic resonance imaging, manual boundary tracing method, ellipsoid formula

10 1. Introduction

Autosomal dominant polycystic kidney disease (ADPKD) is a genetic and systemic 11 12 disease characterized by multiple cysts developing in the kidneys and progressive loss of kidney functions with an increase in total kidney volume (TKV) [1,2]. Currently, 13 14 there is no definitive treatment for this disease [3]. Some preventive measures such as 15 salt restriction, weight control, increasing fluid intake are the first step in treatment. 16 However, some antihypertensive agents, especially angiotensin converting enzyme 17 inhibitors, and lipid-lowering agents are used in the treatment of the disease [4]. The 18 vasopressin-2 receptor antagonist (tolvaptan), which is effective on the 19 pathophysiological mechanism responsible for cyst formation, is one of the pharmacological agents that has been used recently [5]. The Tolvaptan Efficacy and 20 21 Safety in Management of Autosomal Dominant Polycystic Kidney Disease and its 22 Outcomes (TEMPO) 3:4 and 4:4 studies show that the use of tolvaptan slows renal 23 disease progression in patients with advanced ADPKD, and there is a decrease in TKV

in patients receiving tolvaptan after 3 years of follow-up [6,7]. In the TEMPO 3:4 study,
it was stated that it would be appropriate for the patient group aged 18-55 years with a
estimated glomerular filtration rate (eGFR) above 60 ml/min and a TKV above 750 ml
to receive tolvaptan treatment [6]. TKV is used in both treatment decision and followup in ADPKD patients.

6 Magnetic resonance imaging (MRI) is accepted as the gold standard method for TKV 7 measurement in the literature [8,9]. TKV volume can be calculated in two ways in MRI: ellipsoid formula (EF) and manual boundary tracing method (MBTM). The EF is a 8 generally accepted practical volume measurement method of spherical or oval shaped 9 10 structures that is frequently used in daily radiology practice. The MBTM is a standard 11 volume measurement method that can be used to measure the volume of any shaped 12 organ, but requires a longer time [10]. Although MBTM for TKV is the gold standard 13 technique, it is a time-consuming method and also requires special software [10]. Due to these disadvantages, it is difficult to implement in practice. The EF, on the other hand, 14 15 is less time consuming, does not require special software, and is therefore a method preferred by radiologists in daily practice. Repeatability is one of the most important 16 parameters that determine the reliability of different measurement methods. Therefore, 17 18 in this study, it was aimed to investigate the intraobserver and interobserver agreement of the EF and MBTM used in TKV measurement of patients with ADPKD in 19 radiologists with different experience levels. In addition, since the MBTM for TKV is 20 21 considered the gold standard, the correlation of the EF with this method was also evaluated. 22

23

1 2. Materials and methods

2 The study was approved by the Ethics Committee of the Faculty of Medicine of

3 Eskişehir Osmangazi University (Date: 22.12.2021 No:E-25403353-050.99-266323).

4 The study was conducted in accordance with the principles of the Helsinki Declaration.

5 All image data used in this study were obtained from routine imaging at our institution.

6 Datasets were evaluated retrospectively. Therefore, approval and informed consent were

7 not necessary and were waived by our local institutional review board.

8 2.1.Study participants

9 The MRI of ADPKD patients who underwent abdomen MRI between January 2017 and

10 November 2021 for evaluating TKV were evaluated retrospectively. Patients with MRI

11 in which it was not possible to evaluate TKV due to motion artifacts (n=2) or an

12 inappropriate MRI (n=3 not whole kidney in imaging area) were excluded from the

13 study. The MRI scans of the remaining 55 patients were included in the study.

14 2.2.Image acquisition, analysis and interpretation

15 All MRI scans were performed on a 3 T (General Electric) MRI device using a 48-16 channel body coil. Contrast material was not used in any of the patients. Axial plane T1 weighted gradient echo, T2 weighted single shot fast spin echo sequences in the axial, 17 18 coronal and sagittal planes were obtained. The images were evaluated by radiologists using a dedicated workstation (Advantage WorkStation AW 4.7 software, GE 19 20 Healthcare, WI, USA). The measurements were performed by three independent observers (observer 1, an abdominal imaging radiologist with 5 years of experience; 21 22 observer 2, a fourth-year radiology resident; observer 3, a second-year radiology resident) who both performed two measurements for each parameter from which the 23 average values were obtained. To assess intraobserver variability, both observers 24

repeated the measurements again at two week intervals. The volumes of the right and
 left kidneys were calculated separately and then TKV was found by summing them
 (Total 110 kidney in 55 patients, all patients had two kidney, no patient had solitary
 kidney). T2 weighted single shot fast spin echo sequences were used for all
 measurements.

For MBTM, both kidney boundaries were manually drawn on axial plane one-by-one on
each slice (Figure 1). Kidney volumes were calculated from the set of contiguous
images by summing the products of the area measurements within the kidney
boundaries and slice thickness. Kidney volume was obtained by automatically with
software.

11 The recommendation of the Mayo Clinic was used for the EF ($\pi/6$ x Lenght (Coronal

12 Lenght +Sagittal Length)/ $2 \times$ Depth \times Width) (Mayo Clinic (2013). Imaging

13 classification of ADPKD: A simple model for selecting patients for clinical trials

14 [online]. Website https://www.mayo.edu/research/documents/pkd-center-adpkd-

15 classification/doc-20094754 [accessed 28 01 2023). Parameters are obtained from the 4

16 measurements with using the axial, coronal, and sagittal planes. For each kidney, length

17 was measured as the average maximal longitudinal diameter measured in the coronal

and sagittal plane. Width was obtained from the transversal image at maximum

19 transversal diameter, and depth was measured from the same image perpendicular to the

20 width measurement (Figure 2).

21 **2.3.Statistical analysis**

SPSS software v. 22.0 (IBM Corp.) was used for statistical analysis. Normality analysis
was performed by the Shapiro-Wilk test. The mean, standard deviation (SD), minimum

and maximum values were obtained as descriptive statistics of continuous data, and 1 frequency (percentage) values for discrete data. The intraclass correlation coefficient 2 3 (ICC) was used to assess intraobserver and interobserver variability. Based on the 95% confidence interval (CI) of the ICC estimate, values less than 0.5, 0.5 to 0.75, 0.75 to 4 5 0.9, and greater than 0.90 indicate poor, moderate, good, and excellent reliability, 6 respectively. Comparison of two methods for TKV was performed by linear regression 7 for all three observers. 8 3. Results The study included 55 patients, of whom 26 (47.2%) were female and 29 (52.7%) were 9 10 male. The mean age of the patients participating in the study was 47.36 ± 12.28 (25-80) 11 years. The descriptive statistics of TKV calculated using the EF and MBTM, and 12 measured by the first, second and third observers are given in Table 1. ICC (95% CI) indicated excellent agreement between the observers for both two 13 methods (among all observers, p<0.001). Moreover, excellent intraobserver agreement 14 15 was found between all observer measurements either EF or MBTM on ICC (95% CI) (p<0.001). Table 2 and 3 shows detailed information about intraobserver and 16

17 interobservers agreement.

Linear regression analysis was performed for all three observers to assess the correlation
of measurement methods. High correlations were observed for two methods in all 3
observers (For first observer r=0.992, p<0.001; for second observer r=0.975, p<0.001;
for third observer r=0.989, p<0.001) (Figure 3).

22 **4. Discussion**

In this study, we evaluated the intraobserver and interobserver agreement levels and the
correlation between the two methods (EF and MBTM) for determine TKV in ADPKD
patients in radiologists with different experience levels. We found that both the EF and
MBTM had excellent intraobserver and interobserver agreement. The correlation of the
EF with the MBTM, which is considered the gold standard for TKV, was also very
high.

7 In the literature, there are some studies using different radiological methods to calculate 8 TKV volume in ADPKD patients [9]. Ultrasonography (USG); despite its advantages 9 such as being cheap, easily accessible and not containing ionizing radiation, it is not a 10 precise and accurate method that can be used for this purpose [11,12]. Despite the 11 advantage of short time of computed tomography (CT) application, its use in practice is limited (except in patients who cannot undergo MRI) due to ionizing radiation 12 13 exposure, which poses a problem especially with repetitive examinations, and the difficulty in using iodinated contrast material in patients with impaired renal function 14 15 [12]. MRI is the most appropriate imaging method used for this purpose because of its high soft tissue contrast resolution and the ability to easily identify renal borders and 16 17 cysts without the need for contrast material. In the Consortium for Radiologic Imaging 18 Studies of Polycystic Kidney Disease (CRISP) study, it was found that there was 19 differences in TKV in measurements made with contrast and non-contrast T1-weighted images [13]. Today, T2-weighted sequences have replaced T1-weighted sequences due 20 21 to the risk of nephrogenic systemic fibrosis of gadolinium-containing contrast agents and the rapid acquisition of T2-weighted sequences in parallel with recent technological 22 23 developments. In our study, we also performed TKV measurements on T2-weighted 24 sequences.

The gold standard method for TKV is MBTM performed on MR images [10]. In the
literature, studies on this subject have shown that this method has high reproducibility
rates. However, it is a time consuming method and requires a specialized workstation
[14]. Due to their heavy workload, radiologists need a less time-consuming and accurate
method that can be applied in daily practice. For this purpose, studies have been
conducted to evaluate whether the EF can be used due to the short evaluation time
compared to the MBTM.

8 In their study, Higashihara et al. found that intra and interobserver reliabilities in 9 standard TKV and in TKV calculated with EF were highly reliable [14]. Irazabal and 10 co-authors maintain that TKV calculated with the EF is strongly correlated with TKV 11 calculated by the stereological method ($R^2=0.979$) [15]. In our study we found a 12 strongly correlation for all three observers regardless of experience, like this study (For 13 first observer r=0.992, p<0.001; for second observer r=0.975, p<0.001; for third observer r=0.989, p<0.001). In addition to this study, we also found that the 14 15 intraobserver and interobserver agreement of the EF was excellent and independent of experience. Cohen et al. stated the while intraobserver agreement was excellent with the 16 17 semiautomatic MR volumetric method, the interobserver agreement was quite good 18 [16]. They suggested that the reason why the interobserver agreement is lower than the 19 intraobserver agreement is that the reader experiences are different and the workstation formal education is insufficient. We found excellent intra and interobserver agreement 20 21 with both MBTM and EF, and we therefore think that this is independent of experience. Sharma et al., in their study with expert and beginner level observers, they found high 22 23 intraobserver variability in the beginer operator and reported that the measurements should be made by the expert operator [17]. Kidney volumes were performed on T1-24

weighted images in this study. Kidney cysts and their borders are more difficult to
distinguish on T1-weighted images than on T2-weighted images. Therefore, fast T2weighted sequences have been used for this purpose in recent studies. The high
intraobserver variability of the beginner operator may be due to this. Also, the operators
in this study are not radiologists. Non-radiologist operators may not be as familiar with
MR images as radiologists. This may be another reason for the inconsistency with our
study.

8 In recent years, there have been studies conducted with artificial intelligence (AI) applications for automatic kidney segmentation in ADPKD patients. Kline et al. found 9 10 that the AI segmentation system they developed performed equally with the readers 11 [18]. Goel et al. stated that the model-assisted segmentation, which they developed with 12 the deep learning method, requires 51% less time than the manual contour 13 determination method without model support [19]. These studies with AI are very promising for the future; but still, full stomach, full bladder, hemorrhagic renal cysts 14 15 and cysts located at the liver borders are the cause of significant failure [19]. We think that the validity and widespread using of these studies, which are obtained with AI 16 17 application, will take time. It seems that radiologists will spend time measuring volume 18 in ADPKD patients in the near future, as they do today. We did not record the evaluation times for the MBTM and EF, but the average time for the MBTM in the 19 literature is between 28 and 90 minutes [20]. On the other hand, 5-7 minutes are 20 21 reported for the EF [21]. The MBTM requires 4-18 times more time than the EF. According to the results of our study, the EF is a time-effective method that can be used 22 safely by radiologists with different levels of experience. We can also speculate that the 23 24 EF is more preferable among radiologists due to the increasing workload and the

MBTM being the tedious contouring task. Of course, the most important issues are
 repeatability and accuracy. The result of our study may relieve radiologists in this
 preferences.

4 The most important limitation of the study is its retrospective nature. Obtaining data 5 from a single center is another limitation. In our study, all MRI examinations were 6 performed on a 3 T MRI device. Three-tesla scanners have a higher magnetic feld 7 strength and provide higher signal to noise ratio, thus better image quality and cyst 8 contrast [21]. In order for the results of our study to be valid at 1.5 T, it may be 9 necessary to support studies with MRI devices with this magnetic field strength. 10 In conclusion, both of methods (MBTM and EF) using in this study provided excellent intra and interobserver reproducibility. The EF is as accurate and precise as the MBTM 11 12 and it is a reliable method for rapid and easy assessment independent of experience. It can be preferred in radiology departments with heavy workload. 13 14 **Conflict of interest**

15 The authors have no conflicts of interest to declare.

16 **References**

Grantham JJ, Geiser JL, Evan AP. Cyst formation and growth in autosomal
 dominant polycystic kidney disease. Kidney International 1987; 31 (5): 1145 1152. https://doi.org/10.1038/ki.1987.121

Chebib FT, Torres VE. Autosomal Dominant Polycystic Kidney Disease: Core
 Curriculum 2016. American Journal of Kidney Diseases 2016; 67 (5): 792–810.
 https://doi.org/10.1053/j.ajkd.2015.07.037

1	3.	Igarashi P, Somlo S. Genetics and pathogenesis of polycystic kidney disease.
2		Journal of the American Society of Nephrology 2002; 13 (9): 2384–2398.
3		https://doi.org/10.1097/01.asn.0000028643.17901.42
4	4.	Chapman AB, Devuyst O, Eckardt KU, Gansevoort RT, Harris T et al.
5		Autosomal-dominant polycystic kidney disease (ADPKD): executive summary
6		from a Kidney Disease: Improving Global Outcomes (KDIGO) Controversies
7		Conference. Kidney International 2015; 88 (1): 17-27.
8		https://doi.org/10.1038/ki.2015.59
9	5.	Torres VE, Chapman AB, Devuyst O, Gansevoort RT, Grantham JJ et al.
10		Tolvaptan in patients with autosomal dominant polycystic kidney disease. The
11		New England Journal of Medicine 2012; 367 (25): 2407–2418.
12		https://doi.org/10.1056/NEJMoa1205511
13	6.	Torres VE, Meijer E, Bae KT, Chapman AB, Devuyst O et al. Rationale and
14		design of the TEMPO (Tolvaptan Efficacy and Safety in Management of
15		Autosomal Dominant Polycystic Kidney Disease and its Outcomes) 3-4 Study.
16		American Journal of Kidney Diseases 2011; 57 (5): 692–699.
17		https://doi.org/10.1053/j.ajkd.2010.11.029
18	7.	Torres VE, Chapman AB, Devuyst O, Gansevoort RT, Perrone RD et al.
19		Multicenter, open-label, extension trial to evaluate the long-term efficacy and
20		safety of early versus delayed treatment with tolvaptan in autosomal dominant
21		polycystic kidney disease: the TEMPO 4:4 Trial. Nephrology Dialysis
22		Transplantation 2018; 33 (3): 477-489. https://doi.org/10.1093/ndt/gfx043

1	8.	Cavoli GL, Finazzo F, Mongiovi R, Bono L, Ferrantelli A et al. The imaging of
2		total kidney volume in ADPKD. Brazilian Journal of Nephrology 2020; 42 (3):
3		384-385. https://doi.org/10.1590/2175-8239-JBN-2019-0218
4	9.	Magistroni R, Corsi C, Martí T, Torra R. A Review of the Imaging Techniques
5		for Measuring Kidney and Cyst Volume in Establishing Autosomal Dominant
6		Polycystic Kidney Disease Progression. American Journal of Nephrology 2018;
7		48 (1): 67–78. https://doi.org/10.1159/000491022
8	10.	Ozkurt S, Dogan I, Ozcan O, Fidan N, Bozaci I et al. Correlation of serum
9		galectin-3 level with renal volume and function in adult polycystic kidney
10		disease. International Urology and Nephrology 2019; 51 (7): 1191-1197.
11		https://doi.org/10.1007/s11255-019-02156-8
12	11.	O'Neill WC, Robbin ML, Bae KT, Grantham JJ, Chapman AB et al.
13		Sonographic assessment of the severity and progression of autosomal dominant
14		polycystic kidney disease: the Consortium of Renal Imaging Studies in
15		Polycystic Kidney Disease (CRISP). American Journal of Kidney Diseases
16		2005; 46 (6): 1058–1064. https://doi.org/10.1053/j.ajkd.2005.08.026
17	12.	Chapman AB, Wei W. Imaging approaches to patients with polycystic kidney
18		disease. Seminars in Nephrology 2011; 31 (3): 237-244.
19		https://doi.org/10.1016/j.semnephrol.2011.05.003
20	13.	Chapman AB, Guay-Woodford LM, Grantham JJ, Torres VE, Bae KT et al.
21		Renal structure in early autosomal-dominant polycystic kidney disease
22		(ADPKD): The Consortium for Radiologic Imaging Studies of Polycystic
23		Kidney Disease (CRISP) cohort. Kidney International 2003; 64 (3): 1035–1045.
24		https://doi.org/10.1046/j.1523-1755.2003.00185.x

1	14. Higashihara E, Nutahara K, Okegawa T, Tanbo M, Hara H et al. Kidney volume
2	estimations with ellipsoid equations by magnetic resonance imaging in
3	autosomal dominant polycystic kidney disease. Nephron 2015; 129 (4): 253-
4	262. https://doi.org/10.1159/000381476
5	15. Irazabal MV, Rangel LJ, Bergstralh EJ, Osborn SL, Harmon AJ et al. Imaging
6	classification of autosomal dominant polycystic kidney disease: a simple model
7	for selecting patients for clinical trials. Journal of the American Society of
8	Nephrology 2015; 26 (1): 160–172. https://doi.org/10.1681/ASN.2013101138
9	16. Cohen BA, Barash I, Kim DC, Sanger MD, Babb JS et al. Intraobserver and
10	interobserver variability of renal volume measurements in polycystic kidney
11	disease using a semiautomated MR segmentation algorithm. American Journal
12	of Roentgenology 2012; 199 (2): 387-393. https://doi.org/10.2214/AJR.11.8043
13	17. Sharma K, Caroli A, Quach LV, Petzold K, Bozzetto M et al. Kidney volume
14	measurement methods for clinical studies on autosomal dominant polycystic
15	kidney disease. PloS One 2017; 12 (5): e0178488.
16	https://doi.org/10.1371/journal.pone.0178488
17	18. Kline TL, Edwards ME, Fetzer J, Gregory AV, Anaam D et al. Automatic
18	semantic segmentation of kidney cysts in MR images of patients affected by
19	autosomal-dominant polycystic kidney disease. Abdominal Radiology (New
20	York) 2021; 46 (3): 1053–1061. https://doi.org/10.1007/s00261-020-02748-4
21	19. Goel A, Shih G, Riyahi S, Jeph S, Dev H et al. Deployed Deep Learning Kidney
22	Segmentation for Polycystic Kidney Disease MRI. Radiology Artificial
23	Intelligence 2022; 4 (2): e210205. https://doi.org/10.1148/ryai.210205

20. Kline TL, Edwards ME, Korfiatis P, Akkus Z, Torres VE et al. Semiautomated
Segmentation of Polycystic Kidneys in T2-Weighted MR Images. AJR.
American Journal of Roentgenology 2016; 207 (3): 605-613.
https://doi.org/10.2214/AJR.15.15875
21. Gregory AV, Anaam DA, Vercnocke AJ, Edwards ME, Torres VE et al.
Semantic Instance Segmentation of Kidney Cysts in MR Images: A Fully
Automated 3D Approach Developed Through Active Learning. Journal of
Digital Imaging 2021; 34 (4): 773–787. https://doi.org/10.1007/s10278-021-
00452-3

Table 1 Descriptive statistics of TKV

	Observer 1 Mean±SD (cm ³) Min-Max (cm ³)	Observer 2 Mean±SD (cm ³) Min-Max (cm ³)	Observer 3 Mean±SD (cm³) Min-Max (cm³)
First measurement	1714.85 ± 1318.65	1935.80 ± 1437.04	1718.42 ± 1294.40
(EF)	365-6658	296-7039	370-6082
Second	1782.75 ± 1369.74	2008.33 ± 1563.58	1698.42 ± 1235.79
measurement (EF)	350-7073	412-7677	328-5680
First measurement	1855.96 ± 1431.10	1886.89 ± 1425.64	1927.85 ± 1434.78
(MBTM)	410-6971	419-6927	446-6956
Second	1845.53 ± 1410.50	1911.44 ± 1451.55	1980.47 ± 1469.95
measurement	196-6840	412-6970	438-7065
(MBTM)			

3 *TKV, Total Kidney Volume; EF, Ellipsoid Formula; MBTM, manual boundary tracing

⁴ method; SD, standard deviation; Min, minimum; Max, Maximum

1 Table 2 ICC Statistics for intraobserver agreement

	ICC	95% Confidence Interval	P value
Observer 1 (EF)	0.98	0.97-0.99	0.0001
Observer 1 (MBTM)	0.99	0.99-0.99	0.0001
Observer 2 (EF)	0.97	0.96-0.98	0.0001
Observer 2 (MBTM)	0.99	0.98-0.99	0.0001
Observer 3 (EF)	0.99	0.98-0.99	0.0001
Observer 3 (MBTM)	0.99	0.99-0.99	0.0001

³ *ICC, Intraclass correlation coefficient; EF, Ellipsoid Formula; MBTM, manual

4 boundary tracing method

- .

Table 3 ICC Statistics for interobserver agreement

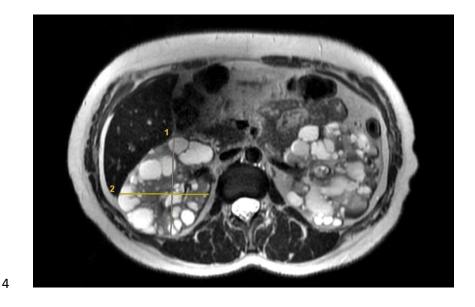
	ICC	95% Confidence Interval	P value
Observer 1-2 (EF)	0.97	0.95-0.98	0.0001
Observer 1-2 (MBTM)	0.98	0.96-0.98	0.0001
Observer 1-3 (EF)	0.98	0.97-0.99	0.0001
Observer 1-3 (MBTM)	0.98	0.98-0.99	0.0001
Observer 2-3 (EF)	0.98	0.96-0.98	0.0001
Observer 2-3 (MBTM)	0.99	0.98-0.99	0.0001

³ *ICC, Intraclass correlation coefficient; EF, Ellipsoid Formula; MBTM, manual

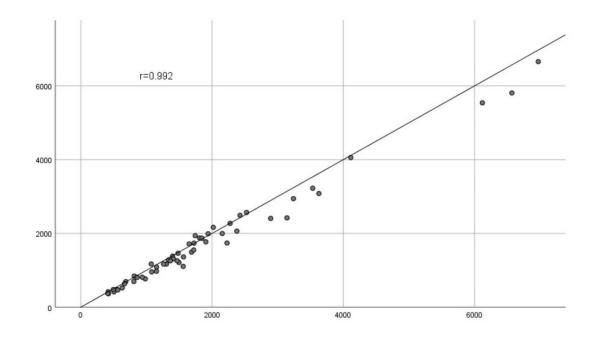
4 boundary tracing method

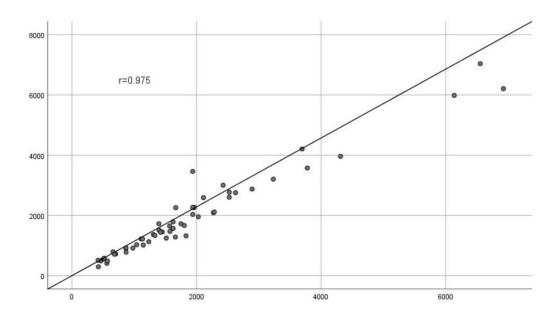


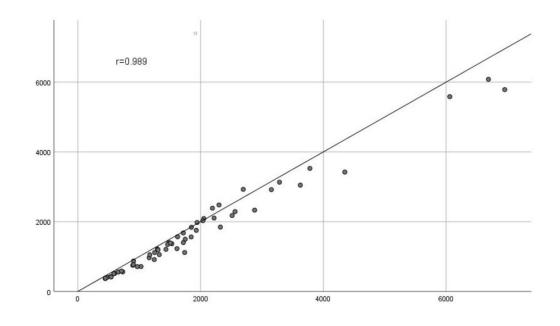
- 2 Figure 1: MBTM for TKV of ADPKD: kidney boundaries manually drawn on axial
- 3 plane T2 weighted MRI



- 5 Figure 2: EF for TKV of ADPKD: The width from the axial plane image at maximum
- 6 transversal diameter, and depth from the same image perpendicular to the width
- 7 measurement
- 8
- 9







- **Figure 3:** Linear regression analysis of measurement methods for all three observers A)
- 3 for first observer, B) for second observer, C) for third observer